REVIEW

The Human Meniscus: A Review of Anatomy, Function, Injury, and Advances in Treatment

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Meniscal injuries are recognized as a cause of significant musculoskeletal morbidity. The menisci are vital for the normal function and long-term health of the knee joint. The purpose of this review is to provide current knowledge regarding the anatomy and biomechanical functions of the menisci, incidence, injury patterns and the advancements in treatment options of meniscal injury. A literature search was performed by a review of PubMed, Google Scholar, MEDLINE, and OVID for all relevant articles published between 1897 and 2014. This study highlights the anatomical and biomechanical characteristics of the menisci, which may be relevant to injury patterns and treatment options. An understanding of the normal anatomy and biomechanical functions of the knee menisci is a necessary prerequisite to understanding pathologies associated with the knee. Clin. Anat. 00:000–000, 2014. © 2014 Wiley Periodicals, Inc.

Key words: meniscus; menisci; knee; anatomy; biomechanics; injury; treatment

INTRODUCTION

Originally described as a vestigial structure (Sutton, 1897), the menisci are now known to be vital for the normal functioning and longevity of the knee joint (Fairbank, 1948; Burr and Radin, 1982; Arnoczky et al., 1988; Arnoczky, 1992; Spilker et al., 1992; Roos et al., 1998, 2001; Rodkey, 2000; McDermott and Amis, 2006). The primary function of the meniscus is to transmit load across the tibiofemoral joint by increasing congruency, thereby decreasing the resultant stress placed on the articular cartilage. The menisci also play a secondary role in shock absorption, stability, lubrication, nutrition, and proprioception to the knee joint (Kettelkamp and Jacobs, 1972; Seedhom, 1976; Seedhom and Hargreaves, 1979; Ahmed and Burke, 1983; Mow et al., 2005; McDermott et al., 2008; Chevrier et al., 2009; Englund et al., 2009).

Injuries to the menisci are recognized as a cause of significant musculoskeletal morbidity (Fox et al., 2012; Rath and Richmond, 2000). As a consequence of its complex anatomical, biomechanical, and functional characteristics, the menisci are prone to damage and injury, particularly in contact-sport activities but also in sedentary young or elderly patients. The challenge remains to develop therapies and techniques that will preserve the menisci’s distinct composition and function.

ANATOMY

Meniscal Etymology

The Latin word meniscus comes from the Greek word mēniskos, meaning “crescent,” diminutive of mēnē, meaning “moon” (Fox et al., 2012).

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Meniscal Phylogeny and Comparative Anatomy

Many species, including all tetrapods, share a genetic lineage reflected by the similar anatomic and functional characteristics and asymmetries of the knee which can be traced back more than 300 million years (Haines, 1942; Mossman and Sargeant, 1983; Dye, 2003). Approximately 1.3 million years ago, the modern patellofemoral joint was established as hominids evolved to a bipedal stance (Tardieu and Dupont, 2001). Tardieu analyzed the ontogenetic transition from occasional bipedalism to habitual bipedalism. The author observed that primates contain a medial and lateral fibrocartilaginous meniscus, with the medial meniscus being morphologically similar in all primates (crescent shaped with two tibial insertions) and the lateral meniscus being more variable in shape (Tardieu, 1999). Unique to Homo sapiens is the presence of two tibial insertions—one anterior and one posterior—indicating the permanent practice of full extension movements of the knee joint during the stance and swing phases of bipedal walking (Retterer, 1907; Vallois, 1914; Ricklin et al., 1983; Preuschoft and Tardieu, 1996; Tardieu, 1999; Beaufils and Verdonk, 2010).

Embryology and Development

The menisci arise from a condensation of the intermediate layer of mesenchymal tissue surrounding the joint capsule. The characteristic shape of the lateral and medial meniscus is achieved between the 8th and 10th week of gestation (Gardner and O'Rahilly, 1968; Gray, 1999). The developing menisci are highly cellular and vascular, with a blood supply extending the entire width and length of the meniscus (Clark and Ogden, 1983). As the fetus continues to develop, there is an increase in collagen content in a circumferential arrangement with a concomitant decrease in cellularity (Clark and Ogden, 1983; Carney and Muir, 1988). Weight-bearing and joint motion during development are important factors in determining the orientation of the collagen fibers. By adulthood, only the peripheral 10 to 30% are vascular (Clark and Ogden, 1983).

Despite these histological changes, the proportion of tibial plateau covered by the corresponding meniscus is relatively constant throughout fetal development, with the medial and lateral menisci covering approximately 51–74% and 75–93% of the surface areas, respectively (Seedhom, 1976; Clark and Ogden, 1983; Fukazawa et al., 2009).

Gross Anatomy

The menisci are crescent shaped wedges of fibrocartilage located on the medial and lateral aspects of the knee (Figs. 1–3). The menisci enable effective articulation between the concave femoral condyles and the relatively flat tibial plateau. The menisci are roughly triangular in cross section, covering one-half to two-thirds of the articular surface of the corresponding tibial plateau. Meniscal horns anchor the menisci to the underlying subchondral bone of the tibial plateau (Messner and Gao, 1998; Villegas et al., 2008) (Fig. 3). These ligamentous structures transmit shear and tensile load from soft tissue into the bone and decreasing contact area (Messner and Gao, 1998). In the medial meniscus, the anterior horn can have a variable site of attachment, into either soft tissue or bone, but a firm bony attachment to the flat intercondylar region of the tibial plateau is most common (Berlet and Fowler, 1998). The posterior horn attaches to the tibia just anterior to the insertion site of the posterior cruciate ligament (PCL) (McKeon et al., 2009; Palastanga and Soames, 2011). In the lateral meniscus, the anterior horn inserts on the tibia in front of the intercondylar eminence, just posterior...
and lateral to the anterior cruciate ligament (ACL) insertion. The posterior horn attaches to the tibia in between the insertion sites of the PCL and the posterior horn of the medial meniscus (Fig. 3) (McKeon et al., 2009). The outer rim of the menisci (also called the red zone) is thick and convex and attached to the knee joint capsule while the inner edge (also called the white zone) is concave, thin and unattached (Fig. 4) (Rath and Richmond, 2000).

Medial Meniscus

The medial meniscus is C-shaped and occupies ~60% of the articular contact area of the medial compartment (Figs. 1, 2, and 3A) (Clark and Ogden, 1983; Arnoczky et al., 1987; Thompson et al., 1991). The posterior horn is significantly wider than the anterior horn, and the anteroposterior dimension is larger than the mediolateral dimension. The anterior horn is

**Fig. 2.** Anatomical photographs of tibial plateau demonstrating the relative size and attachments of the medial and lateral menisci. (A) Superior view. (B) Posterior view. ACL, anterior cruciate ligament; LPRA, lateral meniscus posterior horn attachment; MPRA, medial meniscus posterior horn attachment; PCL, posterior cruciate ligament; SWF, shiny white fibers of posterior horn of medial meniscus. (Reproduced with permission from Johannsen AM, Civitarese DM, Padalecki JR, Goldsmith MT, Wijdicks CA, LaPrade RF. Am J Sports Med, 2012, 40, 2342–2347). [Color figure can be viewed in the online issue, which is available at wileyonlinelibrary.com.]

**Fig. 3.** (A) Anatomy of the meniscus viewed from above (adapted image reprinted with permission from Greis PE, Bardana DD, Holmstrom MC, Burks RT. J Am Acad Orthop Surg. 2002, 10, 168–176; original from Pagnani MJ, Warren RF, Arnoczky SP, Wickiewicz T. The Lower Extremity and Spine in Sports Medicine. 1995, p 581–614, © Mosby. (B) Axial view of a right tibial plateau showing sections of the meniscus and their relationship to the cruciate ligaments. AL, anterior horn lateral meniscus; AM, anterior horn medial meniscus; PCL, posterior cruciate ligament; PL, posterior horn lateral meniscus; PM, posterior horn medial meniscus. (Reproduced with permission from Johnson RJ, Kettelkamp DB, Clark W, Leaverton P. J Bone Joint Surg Am, 1974, 56, 719–729).
firmly attached to the tibia anterior to the ACL, near the intercondylar fossa. The posterior horn is attached immediately anterior to the attachment of the PCL (Figs. 2 and 3). The peripheral border of the medial meniscus merges with the knee joint capsule. The coronary ligament attaches to the meniscus to the upper tibia (Rath and Richmond, 2000).

**Lateral Meniscus**

The lateral meniscus is almost uniformly circular and in contrast to the medial meniscus, it is smaller and considerably more mobile (Figs. 2 and 3A). It also occupies a greater portion of the articular surface (~80% vs. ~60%) (Clark and Ogden, 1983; Amoczky et al., 1987; Thompson et al., 1991). The anterior horn of the lateral meniscus is attached to the intercondylar fossa adjacent to the broad attachment site of the ACL. The posterior horn is attached to the PCL and medial femoral condyle through the meniscofemoral ligaments of Wrisberg (the posterior meniscofemoral ligament) and Humphrey (the anterior meniscofemoral ligament) (Fig. 3A). It is also attached to the popliteus tendon (Last, 1950).

**Biochemistry of the Meniscus**

The meniscus is composed of a dense extracellular matrix (ECM) composed of primarily of water (72%) and collagen (22%), interposed with cells (Ghadially et al., 1983). Other constituents include glucosamino-glycans (17%), DNA (2%), adhesion glycoproteins (<1%), and elastin (<1%) (Herwig et al., 1984; Makris et al., 2011). These proportions vary according to age, injury, or pathological condition (Sweigart and Athanasiou, 2001).

Collagen is the main fibrillar component of the meniscus and varies in amount depending on region within the meniscus. Collagens are primarily responsible for the tensile strength of the meniscus, contributing up to 75% of the dry weight of the ECM (Herwig et al., 1984). In the red zone, type I collagen is predominant (80% composition by dry weight), with other collagen variants (e.g., type II, III, IV, VI, and XVIII) present in less than 1%. Type I collagen fibers are oriented circumferentially, in the deeper layers of the meniscus, parallel to the peripheral border (Fig. 4). In the most superficial region of the menisci, type 1 fibers are oriented in a more radial orientation. Radially positioned "tie" fibers are also present in the deep zone and woven between the circumferential fibers to provide structural integrity (Bullough et al., 1970; Yasui, 1978; Aspden et al., 1985; Beaupre et al., 1986; Arnoczky et al., 1988; Fithian et al., 1990; Skaags and Mow, 1990; Fox et al., 2012). In the white zone, collagen (70% by dry weight) is composed of only two types of collagen - types II (60%) and I (40%) (Cheung, 1987). The collagen fibers are heavily cross-linked and are ideal for transferring vertical compressive load into "hoop stresses" (Voloshin and Wosk, 1983).

Classification of meniscal cells is controversial, with no uniform characterization accepted in the literature (Nakata et al., 2001). Histological examination of the inner white zone of the menisci reveals rounded cells, that behave similarly to fibrochondrocytes or chondrocyte-like cells (Fig. 4) (Verdonk et al., 2005).
The Meniscus: Anatomy, Function, Injury and Treatment

In contrast, the cells of the outer red zone have an oval or fusiform appearance and are classified as fibroblasts (Fig. 4) (Verdonk et al., 2005). A third cell population has been identified in the superficial zone of the meniscus. These cells are flattened and fusiform and lack cell extensions (Van der Bracht et al., 2007). Although the exact purpose of these cells is unknown, it has been suggested that they might be specific progenitor cells with a regenerative capacity (Van der Bracht et al., 2007).

**Vascular Anatomy**

The meniscus is a relatively avascular structure with a limited peripheral blood supply. Branches of the popliteal artery (medial and lateral inferior and middle geniculate arteries) are the major blood vessels that nourish each meniscus. Radial branches from a perimeniscal plexus enter the meniscus at intervals, with a richer supply to the anterior and posterior horns (Fig. 5) (Day et al., 1985). Vascularization is limited to the peripheral 10–25% for the lateral meniscus and 10–30% for the medial meniscus, which has important implications for healing (Arnoczky and Warren, 1982; Danzig et al., 1983; Hamner et al., 2000). Endoligamentous vessels from the anterior and posterior horns travel a short distance into the substance of the menisci to form terminal loops, providing a direct route for nourishment (Danzig et al., 1983). The remainder of the meniscus receives nourishment via synovial diffusion or mechanical motion (Meyers et al., 1988).

**Neuroanatomy**

The meniscus receives innervation via the recurrent peroneal branch of the common peroneal nerve. These fibers follow the blood supply and are found primarily in the peripheral vascular zone covering the outer third of the meniscus (Gardner, 1948; Kennedy et al., 1982). Three distinct mechanoreceptors—Ruffini endings (type 1), Pacinian (type II) and Golgi tendon organs (type III)—have been identified within the meniscus. These neural elements are found in greater concentration in the meniscal horns (particularly the posterior horn), and are important in joint deformation and pressure, tension changes, and neuromuscular inhibition, respectively (Zimny, 1988).

Free nerve endings (nociceptors) can be found in the horns and the outer two-thirds of the body of the meniscus (Wilson et al., 1969; Day et al., 1985; Gronblad et al., 1985; Zimny, 1988; Zimny et al., 1988; Assimakopoulos et al., 1992; Mine et al., 2000).

**BIOMECHANICS AND FUNCTION**

The complex functions of the meniscus are intricately related to their composition, structure, and morphology. The menisci perform many important biomechanical functions. These functions include load transmission (Fairbank, 1948; Walker and Erkman, 1975; Seedhom, 1976; Seedhom and Hargreaves, 1979; Fukubayashi and Kurosawa, 1980; Aspden et al., 1985; Arnoczky et al., 1987), shock absorption (Krause et al., 1976; Kurosawa et al., 1980; Voloshin and Wosk, 1983; Arnoczky et al., 1987; Fithian et al., 1990), stability (Markolf et al., 1976; Fukubayashi et al., 1982; Levy et al., 1982, 1989; Shoemaker and Markolf, 1986), nutrition (Bird and Sweet, 1987, 1988; Renstrom and Johnson, 1990), joint lubrication (Maccoun, 1932; Mac, 1946, 1950; Renstrom and Johnson, 1990), and proprioception (Wilson et al., 1969; Zimny et al., 1988; Assimakopoulos et al., 1992; Jerosch et al., 1996; Messner and Gao, 1998; Saygi et al., 2005; Akgun et al., 2008; Karahan et al., 2010). They also serve to decrease contact stresses and increase contact area and congruency of the knee (Kettelkamp and Jacobs, 1972; Walker and Erkman, 1975).

**Load Transmission**

Studies with long-term follow-up of meniscectomized knees have shown the importance of the meniscus in the functioning of the knee. Fairbank was first to describe the direct load-bearing function of the meniscus by describing the degenerative changes in meniscectomized knees (Fairbank, 1948). Fairbank described narrowing of the joint space, flattening of the femoral condyle, and the formation of osteophytes. Fairbank attributed these changes to the loss of the meniscus (Fairbank, 1948). Since then, several animal and clinical studies have confirmed Fairbank’s thesis that the meniscus is an important protective, load-bearing structure (Walker and Erkman, 1975; Levy et al., 1989; Newman et al., 1989; Fukuda et al., 1992; Mine et al., 2000).
Biomechanical studies have demonstrated that approximately 40–60% of load acting on the extended knee joint is transmitted to the meniscus (65–70% lateral and 40–50% medial) (Shrive et al., 1978; Dudhia et al., 2004). In flexion, this increases up to 90% (Walker and Erkman, 1975). During weight bearing, axial forces compress the menisci, resulting in “hoop” (circumferential) stresses (Voloshin and Wosk, 1983). hoop stresses rely on the conversion of axial force into tensile strain through the circumferential collagen fibers of the meniscus (Fig. 6). The lateral meniscus is displaced more than the medial meniscus during compression, but because of the semilunar anatomy, load is transmitted away from the center of the femoral condyles resulting in tensile stress toward the tibial plateau (Sweigart and Athanasiou, 2001). When standing, the meniscus absorbs most of the load; however, when the knee is in gait or stair climbing, variations in contact stresses occur (Walker and Erkman, 1975; Gilbert et al., 2013). A recent cadaveric study by Gilbert et al. found that during gait, peak contact stresses of the medial plateaus occurred in areas of cartilage-cartilage contact, while on the lateral meniscus peak contact stresses occurred under the meniscus (Gilbert et al., 2013). During stair climb, peak contact stresses of the medial meniscus were located in the posterior aspect of the plateau, under the meniscus. While in the lateral meniscus, during the late phase of stair climb, peak contact stresses were reported in the zone of cartilage-cartilage contact (Gilbert et al., 2013).

Several studies have demonstrated that load is well distributed when the meniscus is intact, however, its removal results in a significant reduction in femoral condyle contact area and a significant increase in contact stress (Kettelkamp and Jacobs, 1972; Fukubayashi and Kurosawa, 1980; Ahmed and Burke, 1983; Radin et al., 1984; Radin and Rose, 1986; Bedi et al., 2012). Several studies have reported that total lateral meniscectomy results in a 40–50% decrease in contact area and an increase in contact stress in the lateral component (200–300% of what is considered normal), which significantly increases the load per unit area and may contribute to accelerated articular cartilage damage and degeneration (Fairbank, 1948;
Stability

The shock absorbing capacity of the menisci has been demonstrated by studies measuring the vibrations in the proximal tibia resulting from gait. From this, it has been shown that shock absorption is approximately 20% less in knees without menisci (Voloshin and Wosk, 1983). This function of the menisci is associated with their viscoelastic properties, the main component of which is the water content of the tissue. Therefore, on impact, shock is absorbed by frictional drag forces, which occur as the fluid escapes the tissue.

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Stability

The incongruous articulation between the convex femoral condyles and flat tibial plateau is ameliorated by the concave-shaped superior surface of each meniscus (Brantigan and Voshell, 1941; Markolf et al., 1976, 1981; Oretorp et al., 1979; Fukubayashi et al., 1982; Levy et al., 1982; Shoemaker and Markolf, 1986; Allen et al., 2000). The firm attachment of the medial meniscus to the tibia contributes to anterior stability of the knee, and is more frequently torn (particularly in ACL-deficient knees) because it is less mobile.

The intact meniscus limits excess motion in all directions, contributing to the stability of the knee joint (Arnoczky, 1992). Although the exact function of the meniscofemoral ligaments (Wrisberg and Humphrey) remains unknown, it is believed that in flexion and internal rotation, the popliteal tendon retracts the posterior horn, thus reducing entrapment of the lateral meniscus between the femur and tibia. Joint stability is further facilitated by the soft tissue structures of the knee joint capsule.

The role that the menisci play in joint stability can best be demonstrated in studies investigating laxity in ACL-deficient, meniscectomized or meniscus-torn knees (Levy et al., 1982; Shoemaker and Markolf, 1986). Findings include greater anterior tibial translation in knees with a sectioned ACL and medial meniscectomy as compared with knees with only ACL sectioning (Bargar et al., 1980). However, ACL sectioning and lateral meniscectomy did not cause an increase in anterior translation in contrast to medial meniscectomy (Levy et al., 1982). Shoemaker and Markolf stated that the posterior horn of the medial meniscus is the most important structure resisting anterior tibial force in the ACL-deficient knee (Shoemaker and Markolf, 1986). Allen et al. showed that the resultant force in the medial meniscus of the ACL-deficient knee increased by 52% in full extension and by 197% at 60 degrees of flexion under a 134-N anterior tibial load (Allen et al., 2000). More recently, Musahl et al. reported that the lateral meniscus plays a major role in the pivot-shift maneuver as lateral meniscectomy increases translation and rotation and increases the pivot shift (Musahl et al., 2010; Pearle, 2011). These significant changes in kinematics in the ACL-deficient knee confirm the important role of the menisci in knee stability.

Joint Lubrication and Nutrition

The menisci may also play a role in the lubrication and nutrition of the knee joint. In a series of studies, MacConaill, reported that the coefficient of friction of the knee joint is increased by 20% following meniscectomy (MacConaill, 1932; Mac, 1946, 1950). The precise mechanism(s) by which lubrication occurs remains unknown; however some authors believe that when the knee is loaded, the menisci compress and circulate synovial fluid into the articular cartilage, reducing the frictional forces during weight-bearing and providing joint nutrition (Mac, 1950; Arnoczky et al., 1988). The system of microcanals within the meniscus that is located close to the blood vessels communicates with the synovial cavity. It is believed that these may provide fluid transport for lubrication and nutrition (Bird and Sweet, 1987, 1988).

Proprioception

The menisci may serve a proprioceptive role as suggested by the presence of mechanoreceptors in the anterior and posterior horns of the menisci (Wilson et al., 1969; Zimny et al., 1988; Assimakopoulos et al., 1992; Jerosch et al., 1996; Messner and Gao, 1998; Saygi et al., 2005; Akgun et al., 2008; Karahan et al., 2010). Quick-adapting mechanoreceptors (e.g., Pacinian corpuscles) are thought to mediate the sensation of joint motion, while slow-adapting receptors (e.g., Ruffini endings and Golgi tendon organs) are believed to mediate the sensation of joint position (Reider et al., 2003). The identification of these neural elements (located mostly in the middle and outer third of the meniscus) indicates that the meniscus is capable of detecting proprioceptive information, thus playing an important afferent role in the sensory feedback mechanism of the knee (Kennedy et al., 1982; Skinner et al., 1984; Aagaard and Verdonk, 1999; Gray, 1999; Karahan et al., 2010).

INJURY

Epidemiology

Meniscal injury is a common source of pain and disability of the knee that is frequently encountered by orthopaedic surgeons, with a mean annual incidence of 60–70 per 100,000 (Hede et al., 1990; Nielson and Yde, 1991; Majewski et al., 2006; Clayton and Court-Brown, 2008). The overall male to female ratio for meniscal tears ranges from 2.5:1 to 4:1, with a peak incidence occurring in males between 21 and 30 years of age and in girls and women between 11- and 20-years old (Baker et al., 1985; Poehling et al., 1990; Greis et al., 2002; Drosos and Pozo, 2004). Medial meniscal tears (particularly in the stable knee or in the chronic ACL-deficient knee) are more commonly involved.
Meniscal tears are more common in association with an acute ACL tear (range, 51–72%) (Poehling et al., 1990). Meniscal tears are generally caused by a combination of axial loading and rotational forces that result in shear load on the meniscus (Browner et al., 2003). Traumatic tears are usually associated with a known insult to the knee and may be isolated or associated with ligament or articular surface injury (Browner et al., 2003). Traumatic tears generally occur in younger, active individuals (Browner et al., 2003). Degenerative tears may reflect cumulative stress and correlate with the presence of associated chrondromalacia (Browner et al., 2003).

Meniscal tears in children are commonly due to trauma or congenital meniscal variants such as a discoid meniscus or meniscal cysts. In adults, meniscal tears are a result of trauma, degenerative disease or a combination of both (Hirschmann and Friederich, 2009; Pujol and Boisrenoult, 2009; Verdonk and Vererfve, 2009). Adult meniscal injuries predominantly involve the medial meniscus, and are often associated with concomitant ligament or cartilage lesions (Pujol and Boisrenoult, 2009; Verdonk and Vererfve, 2009). In addition, tears are more complex in adults as the meniscus undergoes significant degeneration in the course of a lifetime (Pujol and Boisrenoult, 2009). Not surprisingly, there is an increase in the incidence of meniscal tears with increasing age (Pujol and Boisrenoult, 2009).

Symptoms produced by a meniscal tear are typically pain and sometimes mild swelling. Less commonly, “mechanical” symptoms such as locking, catching, grinding, and giving away occur. The frequency and severity of the symptoms varies according to the size and mobility of the meniscal tear (Browner et al., 2003).

**CLASSIFICATION OF MENISCAL TEARS**

Despite the International Society of Arthroscopy, Knee Surgery and Orthopaedic Sports Medicine Committee publishing a standardized and validated system to classify meniscal tears, no classification has been universally accepted by the orthopaedic community (Irrgang et al., 1998, 2006; Crawford et al., 2007; Anderson et al., 2011). Tears are generally classified according to observed tear patterns (seen at arthroscopy) or etiology of the injury and can be described as either full-thickness or partial thickness, depending on vertical depth of the tear (Figs. 7 and 8).

The authors follow the zone classification system devised by Cooper, who provides consistent clinical documentation of meniscal tear patterns and tear locations (Cooper et al., 1990). In this system, the menisci are divided into three radial zones anterior to posterior and four circumferential zones extending from the periphery to the inner aspect of the meniscus (Fig. 9). Tears are further classified according to their morphology and tear pattern relative to the tibial plateau.

The main categories of meniscal tears include vertical longitudinal, radial (transverse), horizontal (cleavage), complex (degenerative), and bucket-handle tears (Greis et al., 2002).

**Vertical Longitudinal Tears**

A vertical longitudinal tear occurs between the circumferential collagen fibers, parallel to the long axis of the meniscus, perpendicular to the tibial plateau, with the tear equidistant from the peripheral edge of the meniscus (Jee et al., 2003). These tears transverse the circumferential collagen fibers, resulting in either two separate pieces of meniscus, or a single portion of meniscus attached to the tibia in only one location (Figs. 7A) (Tuckman et al., 1994; Magee et al., 2002; Fox, 2007). Vertical longitudinal tears are most commonly traumatic in origin and occur more often in younger individuals, with a peak incidence of 21–30 years of age in mean and 11–20 years of age in women (Schepsis and Busconi, 2006). They are noted more frequently medially in isolated cases and laterally in association with ACL tears (Schepsis and Busconi, 2006). The incidence of vertical longitudinal tears ranges from 40 to 84% (Metcalf, 1981; Poehling et al., 1990; Dandy, 1990; Metcalf and Barrett, 2004). As these tears occur between collagen fibers, the biomechanics of the knee is therefore not always disrupted and these
tears may not be symptomatic (Mordecai et al., 2014). Vertical longitudinal tears are commonly repaired because they are amenable to suture fixation.

Radial Tears

Radial (transverse) tears are vertical tears, which often occur at the junction of the posterior and middle thirds and extend from the inner free margin toward the periphery, but can occur at other regions (Figs. 7A). They may also occur in the midbody portion of the lateral meniscus in younger patients. The incidence of radial tears is approximately 14–15% (Helms, 2002; Magee et al., 2002; Harper et al., 2005). Radial tears are typically found in younger patients, with a peak incidence of 11–20 years of age in men and 51–70 years of age in women (Schepsis and Busconi, 2006). Although relatively uncommon, they are usually traumatic with the majority (~79%) occurring in the posterior horn of the meniscus (Helms, 2002; Magee et al., 2002; Harper et al., 2005; Fox, 2007). Radial tear patterns may be associated with ACL rupture involving the posterior portion or meniscal attachment (Wickiewicz, 1990; Vanhoezenaker et al., 2007).

Radial tears disrupt the ability to distribute the hoop stresses associated with weight bearing, and are usually not reparable (Harper et al., 2005; Fox, 2007). Repairs of radial tears that extend to the periphery have the potential to heal because of the peripheral bloody supply (Schepsis and Busconi, 2006). Traditionally, repairs of radial tears were not
Complex tears either have two or more tear configurations or are not easily categorized into a specific type of tear (Jee et al., 2003; Fox, 2007). This is the most common of all meniscal lesions, accounting for nearly 30% of all tears with a peak incidence of 41–50 years of age in men and 61–70 years of age in women (Schepsis and Busconi, 2006). However, atraumatic degenerative flap tears have been identified by magnetic resonance imaging (MRI) and arthroscopy in patients as young as 20 years of age. Complex tears may or may not be associated with any history of trauma and may have an insidious onset. Complex degenerative tears are frequently seen in association with other degenerative changes within the joint. In addition, complex degenerative tears usually have minimal to no healing potential and generally are not amenable to repair (Schepsis and Busconi, 2006).

Bucket-handle Tears

A bucket-handle tear of the meniscus is a vertical or oblique tear with longitudinal extension toward the anterior horn in which the inner fragment is frequently displaced toward the intercondylar notch (Singson et al., 1991). The term bucket-handle is derived from the appearance of the tear, in which the inner displacement fragment of the meniscus resembles a handle, and the peripheral nondisplaced portion has the appearance of a bucket (Singson et al., 1991). Bucket-handle tears often involve the entire meniscus but can also involve only the posterior horn and body or a single horn of the meniscus and are common in ACL deficient knees (Ruff et al., 1998). It is the most common type of displaced "flap" tear, occurring in approximately 10–26% of patients (Lecas et al., 2000; Watt et al., 2000; Ververidis et al., 2006) and more commonly involves the medial meniscus (Magee and Hinson, 1998; Watt et al., 2000; Dorsay and Helms, 2003; Ververidis et al., 2006). The inner flipped portion of the meniscus can remain intact or it can be disrupted.

MECHANISM OF INJURY

The mechanism of injury of meniscal tears can be generally categorized as occurring during a sporting activity (e.g., soccer, rugby football), a nonsporting activity (e.g., squatting), or nonactivity. In a recent study of 392 patients from an unselected population, Drosos and Pozo found that the average age of patients incurred their meniscal injury in a sports-related activity, while over one third (38.8%) occurred due to nonsporting activities and nearly one third (28.8%) of patients could not identify any specific event or incident which resulted in an injury (Drosos and Pozo, 2004).

Injury to the meniscus during sporting activities can be further defined as secondary to contact or noncontact mechanisms, with the latter being the most common. In the young athlete, contact (sports)-related meniscal tears may result from excessive application of force to the meniscus while in older patients, degeneration makes the meniscus particularly susceptible to injury. The mechanism of injury typically involves a twisting or shearing motion, with a varus or valgus force directed to a flexed knee (Hayes et al., 2000). Contact with another player typically does not occur, nor does lunging or landing awkwardly. Patients typically report taking a single "wrong step" (Vanhoenaker et al., 2007). In noncontact (sports)-related injuries, common mechanisms include cutting, decelerating or landing from a jump (Rath and Richmond, 2000).

Age has been suggested as a risk factor of meniscal injury. Drosos and Pozo found that the average age of the sporting, nonsporting and nonactivity groups was 33, 41, and 43 years, respectively (Drosos and Pozo, 2004). The differences may reflect a higher representation of the general population in recreational sports and of age-related degenerative changes within the meniscus, which make it more vulnerable to injury (Drosos and Pozo, 2004). These findings confirm the opinion of other authors, which state that after the
third decade of life, degenerative changes start to diminish the elasticity and increase the susceptibility of the meniscus to injury (Noble and Hamblen, 1975; Smillie, 1978).

Gender has also been suggested to be a risk factor for meniscal injury. Several studies have reported that men are four times more likely to incur a meniscal injury than women (Baker et al., 1985; Casteleyn et al., 1988; Drosos and Pozo, 2004). This may be due to the subtle anatomical and physiological characteristics of the meniscus, differences in normal daily activities, sports participation, prior participation in sports and differences in occupation, which can result in different rates of microtrauma and degeneration of the meniscus (Drosos and Pozo, 2004).

**IMAGING MODALITIES**

**Standard Radiography**

Although unable to demonstrate pathology of the meniscus, radiographs of the knee are able to exclude bony pathologies and assess the concomitant presence of degenerative changes. Standing weight-bearing radiographs (anteroposterior at 0°, posteroanterior at 45° ("Rosenberg view"), lateral, Merchant views) can show a reduction of the joint space width, loose bodies, chondrocalcinosis, osteophytes, subchondral bone cysts, sclerosis, and other degenerative changes (Rosenberg et al., 1988; Maffulli et al., 2010; Robinson, 2010).

**Magnetic Resonance Imaging**

Magnetic Resonance Imaging is a valuable imaging method for diagnosing meniscal tears, with an accuracy range of 82–95% (Mandelbaum et al., 1986; Reicher et al., 1986; Mueller et al., 1997; Yan et al., 2011; Subhas et al., 2012; Sharifah et al., 2013). Accuracy is defined as a measure of closeness in detecting a quantity to that quantity’s actual (true) value. Sensitivity and specificity of MRI are 93 and 88%, respectively for medial meniscal tears, and 79 and 95%, respectively for lateral meniscal tears (Oei et al., 2003). Sensitivity and specificity are statistical measures that describe the proportion of actual positives that are correctly identified and the proportion of negatives that are correctly identified, respectively. Spin-echo or fast spin-echo proton density with or without fat saturation, T1, and gradient echo are the most commonly used sequences (Helms, 2002).

The MRI grading system classifies tears based on their appearance on an MRI scan (Fig. 8). Grade 0 represents an intact, normal meniscus. Grade I and Grade II signals do not intersect the superior or inferior articular surface of the meniscus, but may represent meniscal degeneration. A Grade III signal intersects the superior and/or inferior articular surface of the meniscus and represents a tear (Fig. 8).

**Arthroscopy**

Diagnostic arthroscopy has become the gold standard for assessing meniscal injuries and determining the feasibility of a successful repair (Maffulli et al., 2012). A probe is used to characterize the size of the tear, degree of instability, quality of the tissue and zone of the tear (i.e., red–red, red-white, and white–white) and the width and integrity of the meniscal rim is evaluated (Jackson, 2008). Once the diagnostic arthroscopy is complete, the treating surgeon should determine the appropriate treatment.

**ADVANCES IN TREATMENT**

The goal of surgical intervention for meniscal tears is to relieve pain, facilitate preinjury level daily living activities, and prevent early degeneration of the knee joint. In the past, total meniscectomy was the gold standard because the meniscus was considered a functionless remnant vestige (Sutton, 1897). In his landmark article, Fairbank radiologically examined postmeniscectomized knees, describing the femoral condylar flattening and narrowing of the joint space that occurred over time (Fairbank, 1948). However, despite this evidence, total meniscectomy remained the widespread treatment of meniscal tears until the 1970s.

Over the past four decades, with the general adoption of arthroscopy, there has been an improvement in surgical techniques to assess and treat meniscal pathology. These improvements along with an enhanced understanding of the anatomic structure and biomechanical function of the menisci has led to a shift toward preservation of the menisci to avoid the degenerative results that follow its removal (Jackson, 1968; Appel, 1970; Johnson et al., 1974; Lutfi, 1975; McGinity et al., 1977; Hoch et al., 1983; Northmore-Ball et al., 1983; Voloshin and Wosk, 1983; Allen et al., 1984; Ghosh et al., 1990; Berjon et al., 1991; Abrams et al., 2013). Partial meniscectomy is still indicated if the tear cannot be satisfactorily sutured (Sommerlath, 1991; Shelbourne and Carr, 2003). Meniscal preservation includes leaving small or partial tears, partial meniscectomy and meniscus repair techniques. Meniscal allograft transplantation and the use of synthetic implants have been described in the literature and have shown promising results in symptomatic patients that have undergone a partial, subtotal or total meniscectomy (Brophy and Matava, 2012).

**Meniscal Repair**

Meniscal repair techniques have been developed and refined over the years. A combination of techniques may be used to adequately stabilize a particular meniscal tear. Common to every type of meniscal repair is preparation of the meniscus and the local environment. Any loose or frayed fragments of meniscus should be removed and the opposing edges are rasped to define the meniscal edge and promote the healing response (Ochi et al., 2001; Laible et al., 2013). It is also recommended that abrasion of the local synovium be routinely performed.

Only certain types of tears are feasible for meniscal repair due to the limited vascular supply of the meniscus. Tear morphologies such as flaps, radial tears, and...
Degenerative tears are generally not repaired (Laibl et al., 2013; Taylor and Rodeo, 2013). In a prospective study using second-look arthroscopies, Scott et al. reported the highest rates of healing in menisci that had a narrow peripheral meniscal rim (range 0–2 mm) (Scott et al., 1986). Typically, longitudinal tears that are less than 3 cm in length and within the peripheral zone of the meniscus are amenable to repair (Taylor and Rodeo, 2013). Currently, it is unclear whether the timing of repair affects success (Tengrotenhuyzen et al., 2011; Laibl et al., 2013). Age of patient has been reported to be a factor in capacity to heal. Laibl et al. reported an improved healing response in younger patients following meniscal repair (Laibl et al., 2013). In the event that a ligamentous (e.g., ACL) injury has occurred concomitantly with the meniscal tear, it is recommended that reconstruction be performed to improve functional stability of the knee (Nepple et al., 2012). Meniscal repair in conjunction with ACL reconstruction orthopaedic surgeons can expect an estimated >90% clinical success rate at 2-year follow-up (Warren, 1990; Cannon and Vittori, 1992; Guisasola et al., 2002; Pujol et al., 2008; Pujol and Beaufils, 2009; Toman et al., 2009; Ghodadra et al., 2012; Fu et al., 2013; Yan et al., 2014). Conversely, meniscal reconstruction in the ligamentous stable knee, without concomitant ACL reconstruction resulted in a 50–67% clinical success rate (Cannon and Vittori, 1992; Daniel et al., 1994; Shelbourne and Klotz, 2006). It is believed that simultaneous ACL reconstruction with meniscal repair achieves better meniscal healing because of intra-articular bleeding from the surgically exposed tunnels (Ochi et al., 2001; Guisasola et al., 2002; Scotti et al., 2009) and the improved stability of knee (Shelbourne et al., 1996).

Several repair techniques facilitating suture alone or repair devices has been described in the literature. The inside-out and outside-in techniques use suture that is either first passed on either side of the tear through the meniscus using a cannulated needle and passed out of the joint capsule (inside-out technique) or the other way round (outside-in technique). The main risk of this technique is to cause injury to neurovascular structures and the difficulty in accessing the anterior portion of the medial and lateral menisci (Laible et al., 2013). Newer generation repair devices allow all-arthroscopic meniscal repair by facilitating anchors located outside the joint capsule and sliding knots that can be tensioned by the surgeon for secure tear repair. Meniscal horn tears may be fixed back to the tibial plateau either using suture anchors in the bone or using a transossseous suturing technique with sutures brought through bone tunnels. Typically, postoperative recovery following meniscal repair is slow (approximately 4 months) due to the need to protect the healing tissue. In an attempt to optimize the healing capacity of the meniscus, a number of augmentation techniques have been investigated. These include trephination (Zhang et al., 1995), fibrin clots (Arnoczky et al., 1988; Henning et al., 1990; van Trommel et al., 1998), and platelet-rich plasma (PRP) (Delos and Rodeo, 2011). Trephination connects a meniscal lesion in the avascular zone to the peripheral blood supply via a vascular access channel and allows vascular ingrowth and enhances the healing potential when combined with suture repair of the lesion (Zhang et al., 1995). Autogenous fibrin clots, a precipitated clot material produced by agitation of whole blood, may contain platelet-derived growth factor and fibrinogen that may act as chemotactic and mitogenic stimuli of reparative cells and provide a scaffolding to support a reparative response of meniscal lesions (Arnoczky et al., 1988). PRP may initiate the healing cascade by releasing growth factors from the alpha and dense granules located in the platelet cytoplasm. These growth factors lead to cellular chemotaxis, angiogenesis, collagen matrix synthesis, and cell proliferation (Delos and Rodeo, 2011). Future studies are required to determine the long-term effects of these augmentation techniques on meniscal healing.

Meniscal Allograft Transplantation

Milachowski et al. were the first to publish a clinical study using meniscal allograft transplantation in painful postmeniscectomized patients (Milachowski et al., 1989). Since then, meniscal transplantation has become an accepted management option for select young symptomatic patients who have undergone a subtotal or total meniscectomy (Fig. 10) (Verdonk et al., 2013). Patients who develop symptoms of pain and swelling due to early degenerative changes following meniscectomy are the typical candidates for this procedure.

A study by Verdonk et al, reported that 75–90% of patients experienced fair to excellent functional results after meniscal allograft transplantation (Verdonk et al., 2013). The authors also found that second-look arthroscopies reported good healing of the peripheral rim to the joint capsule in the majority of patients, although shrinkage of the transplant was observed in some cases (Verdonk et al., 2013). The clinical survivorship 10 years postoperatively is estimated to be 70% for medial and lateral allografts (Verdonk et al., 2013). In a systematic review of the literature by Hergan et al., the expected outcome following meniscal allograft transplantation should be a painless knee during activities of daily living. The patients should be informed that expectations of returning to sports should not be overestimated (Hergan et al., 2011). Recovery time is approximately 6 months.

The primary indication for a meniscal transplant is pain localized to the involved compartment (Brophy and Matava, 2012). At the time of transplantation, there should be only mild pre-existing arthrosis and no focal chondral lesion higher than Grade III (Brophy and Matava, 2012; Verdonk et al., 2013). A stable knee joint in correct axial alignment should be ensured. If necessary, ligamentous reconstruction and/or corrective osteotomies should be performed. Axial mal-alignment may result in excessive compression loads on the allograft leading to graft failure (Rijk, 2004). A size-matched meniscus implant with a size tolerance of 5% should be used (Brophy and Matava, 2012). Commonly, the periphery of the
Meniscal allograft is sutured to the remaining peripheral rim or the joint capsule. The meniscal horns are fixed with either small, attached bone plugs (the senior authors’ preference) or soft tissue fixation with sutures (Fig. 10).

Contraindications for allograft implantation are advanced arthrosis, obesity, synovial disease, inflammatory arthritis, significant osteoarthritis (OARSI Grade 3–4), and previous joint infection (Verdonk et al., 2013). Drawbacks include the limited number of available grafts, cost, graft sizing, effects of sterilization and preservation on biomechanical strength of the graft, and the risk of disease transmission (Brophy and Matava, 2012; Verdonk et al., 2013). Currently, no level I evidence exists to support the role of a meniscus transplant in halting the progression of osteoarthritis (Hergan et al., 2011).

### Synthetic Implants

Synthetic scaffolds are emerging as a promising alternative to meniscal allograft transplantation for partial meniscal replacement in symptomatic patients. The Menaflex Collagen Meniscal Implant (Regen Biologics, Hackensack, NJ) and the Actifit polyurethane scaffold (Orteq, London, UK) are currently used in clinical studies outside of the U.S. The goal of these resorbable scaffolds is to allow in-growth of meniscus tissue and thereby create a regenerated meniscus over time formed by host tissue (Verdonk et al., 2013).

The Menaflex is composed of Collagen I isolated from bovine Achilles tendons, treated with hyaluronic acid, chondroitin sulphate, glycosaminoglycans and cross-linked with formaldehyde. The scaffold is sterilized with gamma irradiation. The result is a sponge-like structure with a pore size ranging from 75 to 400 microns (Stone et al., 1997). The surgical technique includes preparation of the implant bed, confirmation of the blood supply, rehydration, and sizing of the implant, followed by the securing of the implant to the remaining meniscus using suture (Stone et al., 1997). The implant requires a meniscal rim and intact anterior and posterior meniscal horns for attachment (Rodkey et al., 1999). Rodkey et al. presented a large randomized trial comparing the collagen meniscal implant with partial medial meniscectomy (Rodkey et al., 2008). The authors of this study were able to demonstrate that patients with prior partial medial meniscectomy regained significantly more of their lost activity and significantly fewer reoperations were necessary (Rodkey et al., 2008). Conversely, patients with an acute trauma to the meniscus without prior surgery did not show a significant difference compared to the control group. Zaffagnini et al. presented a nonrandomized cohort study of 33 patients with meniscal injuries and minimum 10 year follow-up (Zaffagnini et al., 2011). Patients themselves decided if they preferred partial medial meniscectomy alone or with implantation of a collagen meniscal implant. At a minimum of 10 years postop, the patients that underwent scaffold implantation showed significantly lower pain scores, higher activity level and significantly less medial joint space narrowing on radiographs than the control group (Zaffagnini et al., 2011).

The Actifit meniscus implant is a slowly degrading polymer-polyacaprolactone and urethane porous scaffold with high interconnectivity. The scaffold has been shown to improve contact area and pressure in a cadaveric ovine model (Maher et al., 2011). Verdonk
and colleagues were able to demonstrate on MRI 3 months after implantation tissue ingrowth and vascular perfusion in 35 of 43 patients (Verdonk et al., 2011). A second-look arthroscopy 1 year following surgery showed integration of the implant in 43 out of 44 patients. Patients with irreparable medial and lateral meniscal defects showed a statistically significant improvement in pain and activity scores 6 months after implantation of the Actifit scaffold compared to baseline (Verdonk et al., 2012).

Several other implants have been tested in animal studies including implants derived from porcine small intestinal submucosa (Cook et al., 2006), polyacrolein-tactone and hyaluronan-derived polymer reinforced with polyactic acid fibers or polyethylene terephthalate net (Chiari et al., 2006), Kevlar reinforced poly-carbonate-urethane implants (Zur et al., 2011), and ultrahigh-molecular-weight polyethylene fiber reinforced polyvinyl-alcohol hydrogel implants (unpublished data).

The current challenges of implant design are the fixation (particularly of total meniscal implants), the material properties, and surface characteristics. Good fixation of the graft to the tibia and joint capsule is mandatory to minimize extrusion of the implant. The material properties of the implant should be engineered to match the compressive and tensile properties of the native meniscus. The implant surface characteristics are important to minimize chondral damage to the femur und tibia.

CONCLUSIONS

The menisci are integral to the normal function of the knee joint and play an important role in load distribution, shock absorption, stability, lubrication, and proprioception. Injuries to the menisci are recognized as a common cause of significant musculoskeletal morbidity. The unique and complex structure of the menisci makes treatment and repair challenging for the patient, the surgeon and the physical therapist. Preservation of the menisci’s distinctive composition and organization is paramount to knee joint health.

REFERENCES


The Meniscus: Anatomy, Function, Injury and Treatment


